MICROMECHANICAL MODEL OF HYPERELASTIC BEHAVIOUR OF CELLULAR MATERIALS

Małgorzata Janus-Michalska

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SMALL STRAIN ANISOTROPIC ELASTICITY

Stress measures

 \mathbf{T}^{ij} - first Piola-Kirchhoff stress tensor

directions of the initial tangent base vectors in the undeformed state

(nominal stress)

 Π^{ij} - second Piola-Kirchoff stress tensor

directions of tangent base vectors in the deformed state

relation:

 $\mathbf{\Pi} = \mathbf{F}^{-1}\mathbf{T}$

Strain measure physical Green's Lagrangian strain tensor

definition of components:

$$\mathbf{E}_{\mathrm{ii}} \coloneqq \frac{1}{2} \left(\Lambda_i^2 - 1 \right)$$

where:

 $\Lambda_i = \frac{dX_i}{dx_i}$ - relative stretch in the direction of *i* axis

$$\mathbf{E}_{ij} \coloneqq \frac{1}{2} \Lambda_i \Lambda_j \sin \Gamma_{ij}$$

where:

 Γ_{ij} - change of angle between two different *ij* axes deformation is given by deformation gradient $\mathbf{F} \Rightarrow 2\mathbf{E} = \mathbf{F}\mathbf{F}^{\mathrm{T}} - \mathbf{I}$ **Constitutive equations**

neo-Hookean constitutive relationship between Green's strain tensor and the second Piola-Kirchhoff stress tensor

()

the case of small strains :

$$\mathbf{\Pi}(\mathbf{E}) = \frac{\partial \mathbf{\Pi}}{\partial \mathbf{E}} \bigg|_{\mathbf{E}=0} : \mathbf{E} = {}^{0}\mathbf{S} : \mathbf{E}$$

where:

 0 **S** - initial elasticity tensor (initial tangent operator)

MICROMECHANICAL ANALYSIS

Cellular materials



Typical plane structures and representative unit cells

Microstructural deformation - kinematics



$$\mathbf{\varepsilon} = \frac{1}{V} \sum_{A_i} sym(\mathbf{n}_i \otimes \Delta_i) \, dS$$

where: Δ_i - midpoint displacement vector,

- \mathbf{n}_i unit normal to the cell boundary.
- \boldsymbol{V} volume of representative unit cell
- A_i face areas perpendicular to struts *i*.

notation: \mathbf{b}_i^0 -position vectors, $\mathbf{n}_i = \frac{\mathbf{b}_i^0}{|\mathbf{b}_i^0|}$ i = 1, 2, ... n, where: $|\mathbf{b}_i^0| = \frac{L_{0-i}}{2}$.

unit **uniform strain field** on the unit cell ${}^{K}\widetilde{\mathcal{E}}$, K = 1, 2, 3,



where:

 Δ_0 - translational component, ψ - rotation (effect of reorientation) Δ_{0-i} - relative midpoint displacement with respect to node

Mechanical model of cellular skeleton structure

Skeleton material:



Timoshenko beam model

resultant forces for the sets of midpoint displacements $\Delta_i = \Delta_i \begin{pmatrix} K \tilde{\mathcal{E}} \end{pmatrix}$ K = 1, 2, 3

$$\begin{split} ^{K} \tilde{F}_{ni} \left(\xi_{i} \right) & \text{axial force,} \\ ^{K} \tilde{F}_{\tau i} \left(\xi_{i} \right) & \text{transversal force} \\ ^{K} \tilde{M}_{i} \left(\xi_{i} \right) & \text{bending moment functions} \end{split}$$

where:

$$\xi_i$$
 - local coordinate axis for strut i, $\xi_i(0) = 0$, $0 \le \xi_i \le \frac{L_{0-i}}{2}$, i=1,2,...n.

obtained using FEM code.

a, b, c) structure analytical solutions also obtained in Mathcad program.

Microscale

 σ^{s} - stress tensor in each point of beam skeleton structure

Initial stiffness matrix

averaging the strain energy density:

$$\Phi_E = \left\langle {}^s \Phi_E \right\rangle_V = \frac{1}{V} \int_{V_s} \left({}^s \Phi_E \right) dV_s$$

where:

 $\left\langle \ \right\rangle_{\!_{V}}$ - volumetric average in skeleton s taken over V

V- volume of unit cell,

Vs- volume of skeleton in unit cell

stiffness matrix components for equivalent continuum

$${}^{0}S_{IJ} = \frac{1}{V} \left(\frac{\partial^{2} \int \left({}^{s} \Phi_{E} dV_{s} \right)}{\partial \left({}^{I} \varepsilon \right) \partial \left({}^{J} \varepsilon \right)} \right)$$

Kelvin notation (in 6-D space) - tensor representation is 3×3 matrix.

structures a, b, c, - analytical formulae $S_{jklm} = S_{jklm} (L_{o-1}, ... L_{o-i}, ... L_{o-n}, t, \gamma, E_s, v_s)$

structure d - components obtained numerically

a)
$$\mathbf{S} = \begin{bmatrix} \frac{E_s t}{L} & 0 & 0\\ 0 & \frac{E_s t}{L} & 0\\ 0 & 0 & \frac{E_s t^3}{L^3} \end{bmatrix}$$
 b)
$$\mathbf{S} = \begin{bmatrix} \frac{\sqrt{3}E_s t}{(L^2 + 3t^2)} & \frac{\sqrt{3}E_s t}{(L^2 + t^2)} & \frac{\sqrt{3}E_s t}{(L^2 + t^2)} & 0\\ \frac{\sqrt{3}E_s t}{(L^2 + t^2)} & \frac{\sqrt{3}E_s t}{(L^2 + t^2)} & \frac{\sqrt{3}E_s t}{(L^2 + t^2)} & 0\\ 0 & 0 & \frac{\sqrt{3}E_s t^3}{3L(L^2 + t^2)} \end{bmatrix}$$

$$\mathbf{c} \mathbf{s} = \begin{bmatrix} \frac{\sqrt{3}E_{s}t(3L^{2}+2t^{2})}{4L^{3}} & \frac{\sqrt{3}E_{s}t(L^{2}-t^{2})}{4L^{3}} & 0\\ \frac{\sqrt{3}E_{s}t(L^{2}-t^{2})}{4L^{3}} & \frac{\sqrt{3}E_{s}t(3L^{2}+2t^{2})}{4L^{3}} & 0\\ 0 & 0 & \frac{\sqrt{3}E_{s}t}{4L} \end{bmatrix} \quad \mathbf{d} \mathbf{s} = \begin{bmatrix} s_{11} & s_{12} & 0\\ s_{12} & s_{22} & 0\\ 0 & 0 & s_{33} \end{bmatrix}$$

Evaluation of elastic range

energy-based limit condition (Rychlewski) for anisotropic solids on a macroscale

$$\sum_{\alpha=I}^{III} \frac{{}^{\alpha} \Phi_E}{{}^{\alpha} \Phi_E^{\rm cr}} = 1$$

where:

 $^{\alpha}\Phi_{E}^{cr}$ - critical energy density stored in an α eigenstate α = 1,11,111.

 ${}^{\alpha}\Phi_{E}$ - energy density for arbitrary given strain state stored in alfa eigenstate

geometric nonlinarity:

$${}^{\alpha}\Phi_{E}^{\mathrm{cr}} = \lambda_{\alpha} \left({}^{\alpha}\mathbf{E}^{cr} \right)^{2}, \qquad {}^{\alpha}\Phi_{E} = \lambda_{\alpha} \left({}^{\alpha}\mathbf{E} \right)^{2}$$

where:

 $\lambda_{\alpha} - \alpha$ eigenvalue of stiffness matrix, ^{α}E - α strain eigenstate ,

The calculation algorithm for critical energies.

Macroscopic level uniform deformations

$${}^{\mathrm{I}}\tilde{\mathbf{E}} = \left({}^{\mathrm{I}}\tilde{\mathbf{E}}_{x}, {}^{\mathrm{I}}\tilde{\mathbf{E}}_{y}, {}^{\mathrm{I}}\tilde{\mathbf{E}}_{xy}\right) \qquad , \qquad {}^{\mathrm{II}}\tilde{\mathbf{E}} = \left({}^{\mathrm{II}}\tilde{\mathbf{E}}_{x}, {}^{\mathrm{II}}\tilde{\mathbf{E}}_{y}, {}^{\mathrm{II}}\tilde{\mathbf{E}}_{xy}\right), \qquad {}^{\mathrm{III}}\tilde{\mathbf{E}} = \left({}^{\mathrm{III}}\tilde{\mathbf{E}}_{x}, {}^{\mathrm{III}}\tilde{\mathbf{E}}_{y}, {}^{\mathrm{III}}\tilde{\mathbf{E}}_{yy}\right)$$

Microscopic level

forces obtained from numerical solution for unit cell skeleton structure: ${}^{\alpha}\tilde{F}_{in}$, ${}^{\alpha}\tilde{F}_{i\tau}$, $\alpha = I,II,III$.

limit condition for skeleton structure :

$$\max_{i} \left({}^{\alpha} \sigma_{x}^{s} \right) = {}^{\alpha} k {}^{\alpha} \tilde{\sigma}_{x}^{s} = {}^{\alpha} k \max_{i} \left(\left| \frac{{}^{\alpha} \tilde{F}_{in}}{A} \right| + \left| \frac{{}^{\alpha} \tilde{F}_{i\tau} l_{i}}{J} \frac{t}{2} \right| \right) = R_{e}^{s} \qquad \alpha = I, II, III \qquad i = 1, 2, ... n$$

scalar multipliers and critical eigenstrains defined :

$${}^{\alpha}k := \frac{R_e^s}{{}^{\alpha}\tilde{\sigma}_x^s} \qquad {}^{\alpha}\mathbf{E}^{cr} = {}^{\alpha}k \cdot {}^{\alpha}\tilde{\mathbf{E}}$$

Homogeneous deformations

A) uniaxial load

in tensial and compressive range

$${}^{A}\mathbf{F} = \begin{bmatrix} {}^{A}\Lambda_{x} & 0 \\ 0 & {}^{A}\Lambda_{y} \end{bmatrix} \qquad \text{where:} {}^{A}\Lambda_{y} = \sqrt{\frac{s_{12} + s_{22} - s_{12}\left({}^{A}\Lambda_{x}\right)^{2}}{s_{22}}}$$



B) biaxial load

in tensial and compressive range

C) simple shear deformation

 ${}^{\mathrm{C}}\mathbf{F} = \begin{bmatrix} 0 & \Gamma \\ 1 & 0 \end{bmatrix}$



Table 1. Specification of microstructure

type	Geometric parameters	Skeleton material
	of skeleton [mm]	parameters
a)	$L_{01}=L_{02}=L_{03}=L_{04}=20$, t=2.0	E _S =2GPa, v _S =0.33, R _e =200 MPa
b)	$L_{01}=L_{02}=L_{03}=L_{04}=L_{05}=L_{06}=20$, t=2.0	E _S =2GPa,v _S =0.33, R _e =200 MPa
C)	$L_{01}=L_{02}=L_{03}=20$, t=2.0	E _S =2GPa,v _S =0.33, R _e =200 MPa
d1)	$L_{01}=L_{02}=1.5$, $L_{03}=1.5$, $t=0.15$, $\gamma=80^{0}$	E _S =10GPa, v _S =0.3, R _e =25 MPa
d2)	$L_{01}=L_{02}=1.575, \ L_{03}=1.575, \ t=0.15, \ \gamma=70^{0}$	E _S =10GPa, v _S =0.3, R _e =25 MPa
d3)	$L_{01}=L_{02}=1.5$, $L_{03}=3.0$, t=0.15, $\gamma=60^{0}$	E _S =10GPa, v _S =0.3, R _e =25 MPa



















B) Biaxial tension-compression test































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Conclusions

- cellulars reveal nonlinear behaviour in elastic range
- structural topology, structural elements stiffnesses influence nonlinear path
- type of material by proportion Re/Es determines the elatic range
- effect of nonlinearity is dependent on type of loading
- the model based on micromechanics requires experimental verification before application

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